# Implementation and Evaluation of a Semi-Automatic Tumor Segmentation Method Master's Thesis Final Presentation

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# Outline

Motivation

Methods

Proposed Segmentation Method

Implementation

Results

Outlook

Summary

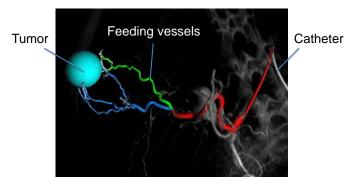


# **Motivation**

June 1, 2015 | J. Glasbrenner | Pattern Recognition Lab (CS 5) | Semi-Automatic 3D Tumor Segmentation Method

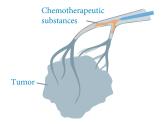


#### C-arm CT imaging with 3D reconstruction



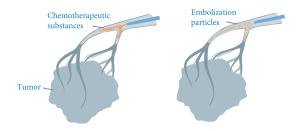
#### Vessel tree and corresponding ROI (cyan sphere)





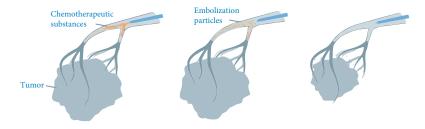
#### Schematic TACE for hepatocellular carcinoma (HCC)





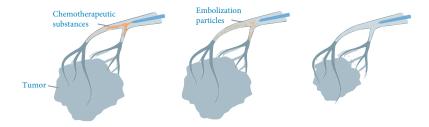
#### Schematic TACE for hepatocellular carcinoma (HCC)





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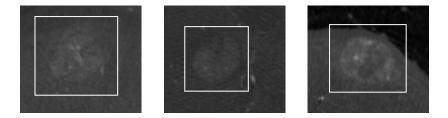


Schematic of the TACE for hepatocellular carcinoma (HCC).  $\Rightarrow$  Goal: Fast and accurate segmentation of various types of tumors



# **Challenges of Tumor Segmentation**

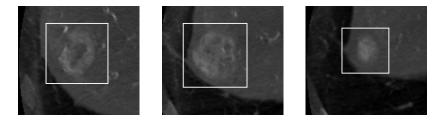
- High diversity no typical shape
- Intensity overlaps between tumor and surrounding tissue
- · Different intensity patches necrotic regions





### Challenges of Tumor Segmentation (cont.)

#### Appearance of a tumor may even vary within different slices





## Automatic vs. Interactive Segmentation

#### Automatic segmentation

- Requires a large ground truth database
- "Semantic-gap" problem

#### Interactive segmentation

- Requires a large amount of user interaction
- Interobserver-variability



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#### Automatic segmentation

- Requires a large ground truth database
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#### Interactive segmentation

- Requires a large amount of user interaction
- Interobserver-variability

 $\Rightarrow$  Solution: Interactive segmentation with automatic initialization



# **Methods**



# **GrowCut Segmentation**

- $\Rightarrow$  Based on cellular automaton theory
- $\Rightarrow$  Discrete in space and time
- $\Rightarrow$  Voxels are treated as cells



# **GrowCut Segmentation**

- $\Rightarrow$  Based on cellular automaton theory
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A cellular automaton is a quad-tuple

$$\boldsymbol{A} = (\boldsymbol{P}^n, \boldsymbol{S}, \boldsymbol{N}, \boldsymbol{\delta})$$

- P<sup>n</sup>: Cellular space
- S: State set
- N: Neighborhood system
- $\delta$ : Local transition rule



- $\Rightarrow$  Based on cellular automaton theory
- $\Rightarrow$  Discrete in space and time
- $\Rightarrow$  Voxels are treated as cells

State of each cell p in cellular space  $P^n$  is a triplet

$$S_{p} = (I_{p}, \theta_{p}, \boldsymbol{c}_{p})$$

- *l<sub>p</sub>*: Label of current cell *p*
- $\theta_p$ : Strength of current cell p
- cp: Feature vector



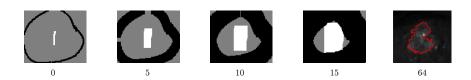
- $\Rightarrow$  Based on cellular automaton theory
- $\Rightarrow$  Discrete in space and time
- $\Rightarrow$  Voxels are treated as cells

Initialization of the cellular automata (CA)

- Unlabeled voxels:
- Foreground voxels:
- Background voxels:
- $\begin{array}{ll} l_{\rho}=0, & \theta_{\rho}=0.0, & \boldsymbol{c}_{\rho}=i_{\rho} \\ l_{\rho}=1, & \theta_{\rho}=1.0, & \boldsymbol{c}_{\rho}=i_{\rho} \end{array} \end{array}$
- $l_{p} = -1, \ \theta_{p} = 1.0, \quad c_{p} = i_{p}$



 $\Rightarrow$  User defined seeds expand over the image

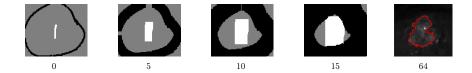




- $\Rightarrow$  User defined seeds expand over the image
- $\Rightarrow$  Cells try to occupy their neighbors iteratively

Attacking strength  $\theta$  of neighboring cell q is weighted by

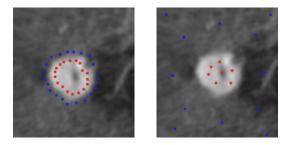
$$g_{\textit{lin}}(oldsymbol{c}_{
ho},oldsymbol{c}_{q}) = 1 - rac{\|oldsymbol{c}_{
ho}-oldsymbol{c}_{q}\|_{2}}{c_{max}} \geq 0$$





### **User Interaction Patterns**

Problem: How to place the seeds efficiently?

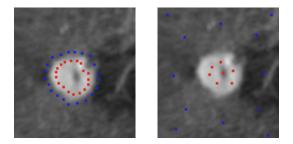


- Volume seeds yield better results than surface seeds [Mo10]
- The more seeds the higher the segmentation quality [Mo10]



### **User Interaction Patterns**

• Problem: How to place the seeds efficiently?



- Volume seeds yield better results than surface seeds [Mo10]
- The more seeds the higher the segmentation quality [Mo10]
- $\Rightarrow$  Solution: Automatically compute a 3D seed template



# **Automatic Initialization**

- $\Rightarrow$  3D seed template...
  - ... maximizes amount of initial seeds
  - ... spreads seeds throughout the volume
  - ... reduces the uncertainty of the user



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- ⇒ Utilize Gaussian Mixture Model
  - Calculate an optimal threshold  $\delta_{opt}$  to compute a seed template



# **Automatic Initialization**

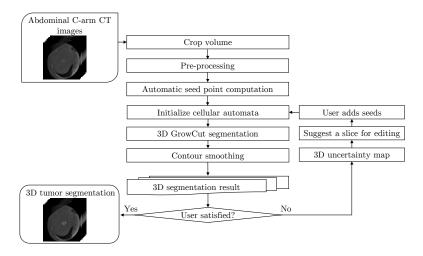
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  - ... maximizes amount of initial seeds
  - ... spreads seeds throughout the volume
  - ... reduces the uncertainty of the user
- ⇒ Utilize Gaussian Mixture Model
  - Calculate an optimal threshold  $\delta_{opt}$  to compute a seed template
  - Initialize seeds with plausible strength  $\theta_p$



# **Proposed Segmentation Method**

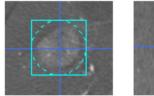


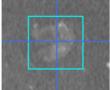
# **Overall Workflow**

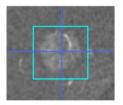




#### **Volume of Interest**

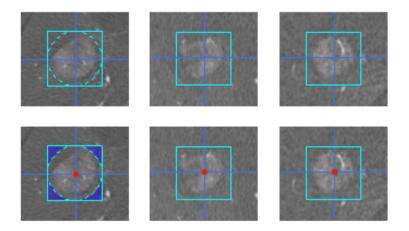






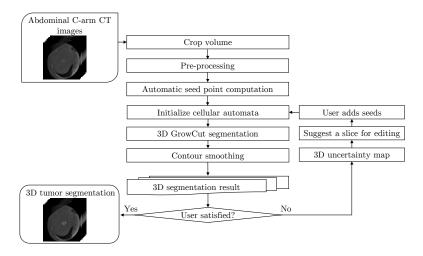


#### **Volume of Interest**



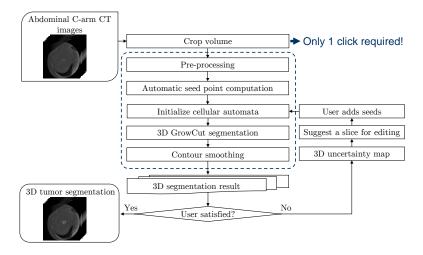


# **Overall Workflow**



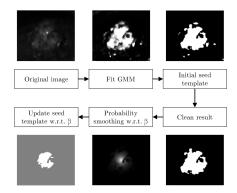


# **Overall Workflow**





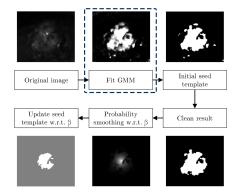
#### **Automatic Initialization - Workflow**



#### 2D example of the procedure of automatized seed point calculation



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#### 2D example of the procedure of automatized seed point calculation



- $\Rightarrow$  Weighted sum of Gaussian distributions
- $\Rightarrow$  All mixing weights add up to one

$$egin{aligned} p(oldsymbol{x}_i) &= \sum_{k=1}^{K} p_k \, \mathcal{N}(oldsymbol{x}_i | \mu_k, oldsymbol{\Sigma}_k) \ &\sum_{k=1}^{K} p_k = 1 \end{aligned}$$

- *p<sub>k</sub>*: The K mixture weights (priors)
- x<sub>i</sub>: Feature vector
- $\mu_k$ : The K means
- $\Sigma_k$ : The *K* covariance matrices



 $\Rightarrow$  weighted sum of Gaussian distributions  $\Rightarrow$  all mixing weights add up to one

$$p(\mathbf{x}_i) = p_1 \mathcal{N}(\mathbf{x}_i | \mu_1, \mathbf{\Sigma}_1) + p_2 \mathcal{N}(\mathbf{x}_i | \mu_2, \mathbf{\Sigma}_2)$$

foreground background

- *p<sub>k</sub>*: the K mixing weights
- *x<sub>i</sub>*: feature vector ⇒ image intensities
- $\mu_k$ : the K means
- **Σ**<sub>k</sub>: the *K* covariance matrices



 $\Rightarrow$  Goal: Assign each pixel a probability that it belongs to the tumor

- Iteratively with Expectation Maximization (EM) algorithm
- · Maximizes the likelihood of the data given the GMM

$$\operatorname*{argmax}_{\theta} \sum_{i=1}^{m} \log p(x_i|\theta)$$



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Parameters to fit to image data:

- Mean  $\mu_k$
- Covariance  $\Sigma_k$
- Mixing weight pk

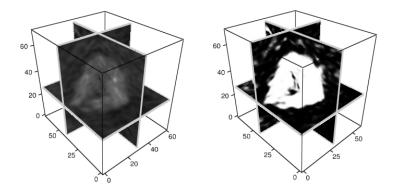


## Gaussian Mixture Model: EM

- 1. Initialize parameters  $\mu_k$ ,  $\Sigma_k$  and  $p_k$
- 2. Step 1: (E step) Given parameters, assign each pixel *x<sub>i</sub>* a probability for each distribution k
- 3. Step 2: (M step) Given probabilities, update parameters  $\mu_k$ ,  $\Sigma_k$ ,  $p_k$  for each distribution k
  - no closed form solution  $\rightarrow$  iterative scheme

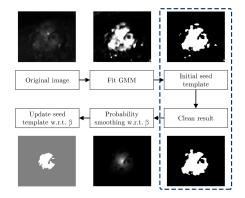


## **Initialization - 3D Probability Map**





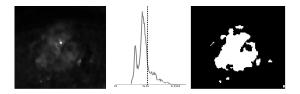
## **Automatic Initialization - Workflow**



#### 2D example of the procedure of automatized seed point calculation



## **Initialization - Seed Template**

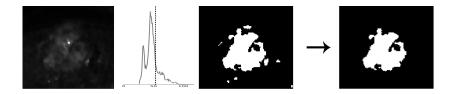


Optimal threshold  $\delta_{opt}$  is the average of the means  $\mu_k$ 

$$\delta_{opt} = \frac{1}{K} \sum_{k=1}^{K} \mu_k$$



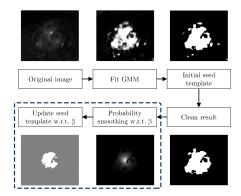
## **Initialization - Seed Template**



- Morphological erosion would erode seed template
- · Maximum of extracted regions accounted as tumor
- Remove all outliers smaller than the mean size of all regions



## **Automatic Initialization - Workflow**



#### 2D example of the procedure of automatized seed point calculation



## **Initialization - Probability Smoothing**

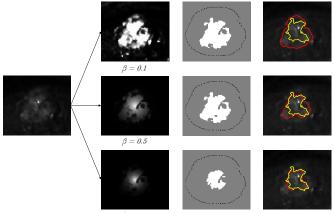
- $\Rightarrow$  Probability being tumor proportional to distance from the VOI center
  - Smooth probabilities far from the VOI center

$$p_{k_{smoothed}} = \exp\left(-\beta(\|u-v\|)^2\right)$$

- u: arbitrary voxel
- v: VOI center



## **Initialization - Probability Smoothing**

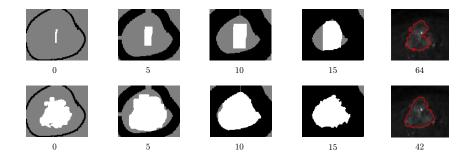


 $\beta = 0.9$ 

#### Influence of the probability smoothing illustrated for an axial slice

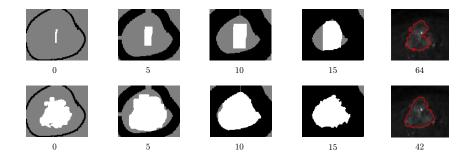


## **Comparison - Label Propagation**





## **Comparison - Label Propagation**

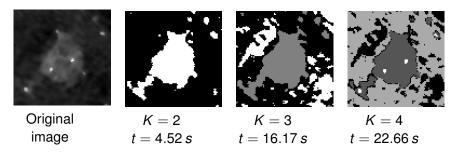


#### $\Rightarrow$ modified method performes better and converges faster



## Number of GMM Components

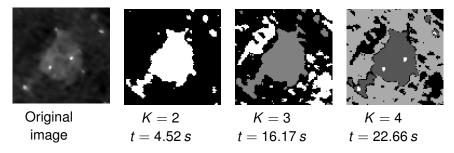
 $\Rightarrow$  Empirically set to K = 2 compontents





## Number of GMM Components

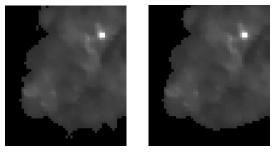
- $\Rightarrow$  Empirically set to K = 2 compontents
  - Computation time increases with K
  - Foreground seeds only change slightly





## **Segmentation Contour Smoothing**

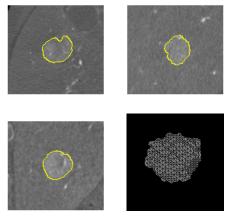
- Smooth ragged segmentation countour
- Morphological operation: binary opening
- Structureing element: 3D sphere



Contour smoothing shown in an axial slice



## **3D Segmentation Result**



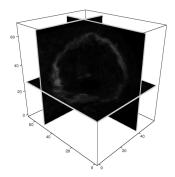
#### 3D segmentation example



## Workflow - Editing of the Segmentation

Segmentation uncertainty: number of label changes per cell

- Store # label changes per cell during propagation process
- · Normalize to maximum number of label changes

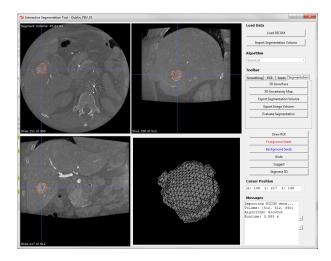




## Implementation



## **Interactive Segmentation Tool - GUI**





## Implementation

### Python

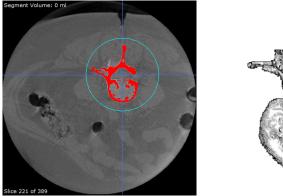
- Concise syntax  $\Rightarrow$  Code reuse
- Cython: Interface with fast C/C++ code
- WinPython: Scientific standalone Python distribution

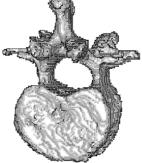
## SciPy/NumPy

- NumPy: powerful N-dimensional array object
- Scikit-learn for machine learning algorithms
- Scikit-image for image processing algorithms



## **Interactive Segmentation Tool - Capabilities**





#### Segmentation of a vertebra



## **Results**



## **Quantitative Evaluation**

- No manually drawn seeds used
- · Ground truth via manual annotation by a clinical expert

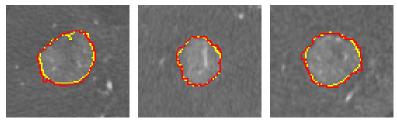
Segmentation algorithm	ARI (%)	DC (%)	MI (%)	RAVD (%)
Proposed method	80.58	85.32	68.88	-0.18
Original GrowCut	72.96	78.46	63.00	-0.26
Random Walker	51.12	57.34	45.46	-0.52
Seeded Watershed	53.28	59.44	47.04	-0.46

Table: Averaged segmentation results for all datasets



## **Segmentation Results**

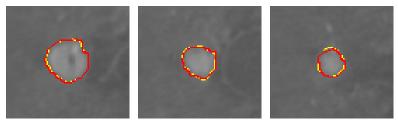
#### Large intensity overlap between cancerous and healthy tissue



Segmentation result of proposed method (yellow) and ground truth (red)



#### Homogenous intensity distribution $\rightarrow$ clear borders

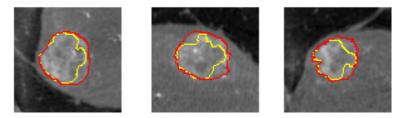


Segmentation result of proposed method (yellow) and ground truth (red)



#### Necrotic tumor $\rightarrow$ inhomogeneous intensities

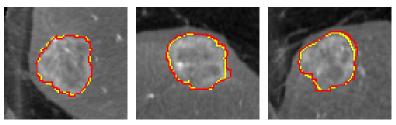
Algorithm might stop label propagation at necrotic borders



# Segmentation result of original GrowCut (yellow) and ground truth (red)



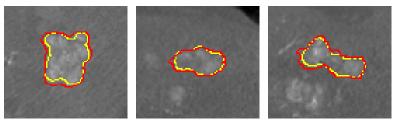
#### Necrotic tumor, inhomogeneous intensities



# Segmentation result of proposed method (yellow) and ground truth (red)



Arbitrary shape with proliferations



# Segmentation result of proposed method (yellow) and ground truth (red)



# **Outlook**



## Outlook

### Extend segmentation method

- · Parallelization of segmentation algorithm on the GPU
- Seperate segmentation of necrotic regions for further investigations

### Extend evaluation

- Sensitivity to user interaction w.r.t. the VOI placement
- Evaluation on a larger ground truth database



# Summary



## Summary

Fast and reliable tumor segmentation is important for

- Quantitative therapy monitoring, e.g. after TACE
- Efficient planing of follow-up treatments

#### An extention of the CA based segmentation algorithm

- · Is realized with a probabilistic model: GMM
- Reduces user interaction to a minimum only one click
- Reduces uncertainty of the user
- Reduces runtime of the overall segmentation process



Thank you for your attention!



## **Bibliography I**

Vezhnevets, Vladimir and Konouchine, Vadim GrowCut: Interactive multi-label ND image segmentation by cellular automata.

Graphicon, 2005.

Moschidis, E. and Graham, J.

A Systematic Performance Evaluation of Interactive Image Segmentation Methods Based on Simulated User Interaction. IEEE international conference on Biomedical imaging, 2010.